



## Article

# Age-Related Modifications of Electroencephalogram Coherence in Mice Models of Alzheimer's Disease and Amyotrophic Lateral Sclerosis

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**Abstract:** Evident similarities in pathological features in aging and Alzheimer's disease (AD) raise the question of a role for natural age-related adaptive mechanisms in the prevention/elimination of disturbances in interrelations between different brain areas. In our previous electroencephalogram (EEG) studies on 5xFAD- and FUS-transgenic mice, as models of AD and amyotrophic lateral sclerosis (ALS), this suggestion was indirectly confirmed. In the current study, age-related changes in direct EEG synchrony/coherence between the brain structures were evaluated. Methods: In 5xFAD mice of 6-, 9-, 12-, and 18-month ages and their wild-type (WT<sub>5xFAD</sub>) littermates, we analyzed baseline EEG coherence between the cortex, hippocampus/putamen, ventral tegmental area, and substantia nigra. Additionally, EEG coherence between the cortex and putamen was analyzed in 2- and 5-month-old FUS mice. Results: In the 5xFAD mice, suppressed levels of inter-structural coherence vs. those in WT<sub>5xFAD</sub> littermates were observed at ages of 6, 9, and 12 months. In 18-month-old 5xFAD mice, only the hippocampus ventral tegmental area coherence was significantly reduced. In 2-month-old FUS vs. WT<sub>FUS</sub> mice, the cortex–putamen coherence suppression, dominated in the right hemisphere, was observed. In 5-month-old mice, EEG coherence was maximal in both groups. Conclusion: Neurodegenerative pathologies are accompanied by the significant attenuation of intracerebral EEG coherence. Our data are supportive for the involvement of age-related adaptive mechanisms in intracerebral disturbances produced by neurodegeneration.

**Keywords:** aging; 5xFAD mice; FUS mice; electroencephalogram; coherence; cortex; hippocampus; putamen; ventral tegmental area; substantia nigra



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## 1. Introduction

Similar abnormalities observed in Alzheimer's disease (AD) and aging [1] are suggested to be associated with disturbances in the functioning of neuronal networks in different brain structures or between them [2–6]. Some adaptive mechanisms preventing the functional decline during aging [7] are assumed to be involved in AD-associated processes [8]. Network alterations, in turn, are accompanied by evident changes in oscillatory features generated by the affected circuits [9,10]. Thus, electroencephalogram (EEG) recordings from various brain structures at different ages are expected to be a useful tool for the analysis of a role for adaptive mechanisms in the development of cerebral decline during the combined influence of AD and aging. Indeed, in previous studies on six- and twelve-month-old 5xFAD mice (an AD model) analyzing the frequency spectra of EEGs simultaneously recorded from cortical and subcortical areas, we assumed that

the results might be explained by an involvement of adaptive/compensatory mechanisms in age-related AD pathology [11,12]. In two- and five-month-old FUS mice (a model of amyotrophic lateral sclerosis, ALS), the obtained data were in line with this suggestion [13]. However, relative changes in the frequency spectra of EEG recorded from different cerebral structures are indirect characteristics of their interrelations, whereas a coherence/synchrony of appearance of instantaneous values for EEGs [14] has been shown to be a direct and effective measure of “functional connectivity” in normal and diseased brains [15–18]. In particular, initial dysfunctions in cortical circuits have been shown to possibly initiate the ALS onset and drive its progression [19], whereas phasic changes in the functioning of neuronal circuits may characterize their ability to adapt as ALS develops [20]. Finally, the interaction of circuits with different connectivity and synchronized activities has been suggested to be involved in neurodegenerative and adaptive/compensatory changes in ALS [21,22].

To analyze an involvement of adaptive/compensatory processes in interrelations between AD and aging [7,8], we measured the levels of baseline EEG coherence between the cortex (MC), hippocampus (HPC)/striatum (putamen, Pt), ventral tegmental area (VTA), and substantia nigra (SN) in six-, eight-, twelve-, and eighteen-month-old 5xFAD mice versus their wild-type (WT<sub>5xFAD</sub>) littermates. In this study, coherence between EEGs from cortical and subcortical areas and from those containing dopamine neurons (VTA and SN) was measured given the evidence about the losing of these neurons in both AD groups [23], in particularly, in 5xFAD mice [11], and in WT<sub>5xFAD</sub> (C57BL/6J) mice [24]. Additionally, we measured the levels of baseline EEG coherence between MC and Pt in two- and five-month-old FUS mice versus WT<sub>FUS</sub> littermates with symmetrically implanted electrodes into these brain areas to control possible interhemispheric differences observed in normal and ALS-affected brains [25]. EEG coherence between MC and Pt is analyzed in this study because of an evolvement of basal ganglia–cortical functional connectivity at both normal development and pathological disturbances associated with basal ganglia dysfunctions [26].

## 2. Materials and Methods

In the “AD” groups, we used male transgenic mice with five familial AD mutations maintained on a C57BL/6J genetic background (5xFAD mice) at ages of 6, 9, 12, and 18 months ( $n = 11, 9, 9,$  and  $7$ , respectively) and non-transgenic wild-type (WT<sub>5xFAD</sub>) littermates ( $n = 14, 8, 7,$  and  $7$ , respectively). In the “ALS” groups, male transgenic mice with truncated human FUS lacking a nuclear localization signal maintained on the CD-1 genetic background (FUS mice,  $\Delta$ FUS(1-359)) at ages of 2 and 5 months ( $n = 8$  and  $6$ , respectively) and WT<sub>FUS</sub> littermates ( $n = 6$  and  $7$ , respectively) were used in this study. All mice were originally obtained from the Center for Collective Use of the Institute of Physiologically Active Compounds RAS (Chernogolovka, Russian Federation). Mice were housed in a standard environment (12 h light/dark cycle, 22–25 °C RT, 50–55% relative humidity) with food and water ad libitum. The procedures were carried out in compliance with the principles enunciated in the Directive 2010/63/EU on the protection of animals used for scientific purposes, and approved by the local institute’s ethics review committee. All efforts were made to minimize the number of animals and their suffering.

### 2.1. Implantation of Electrodes

Each mouse was narcotized by subcutaneous injection of the mixture of tiletamine/zolazepam (25 mg/kg, Zoletil<sup>®</sup>, Virbac, France) and xylazine (2.5 mg/kg, Rometar<sup>®</sup>, Bioveta, Czech Republic). In the 5xFAD mice, EEG recording electrodes were positioned in the left motor cortex and dorsal hippocampus (MC and HPC; AP: +1.1; ML: 1.5; DV: –0.75 and AP: –2.8; ML: –2.7; DV: –1.7 mm, respectively) or putamen (Pt; AP: +1.1; ML: 1.5; DV: –2.75 mm, in “12-month” group), in the left ventral tegmental area (VTA; AP: –3.1; ML: –0.4; DV: –4.5), and in the right substantia nigra (SN; AP: –3.2, ML: +1.3, DV: –4.3) accordantly with the mouse brain atlas [27], where AP, ML, and DV are the distances from

the coronal suture, midline suture, and skull surface, respectively). Within the brain areas analyzed in this study, the opposite hemisphere for SN was chosen to exclude possible mutual damage during electrode implantations in the same hemisphere because of SN proximity to VTA. Furthermore, it is well known that the contralateral SN is the dominant source of DA in the opposite hemisphere.

Two varnish-insulated nichrom wires (100  $\mu\text{m}$  in diameter) glued together (3M Vet-bond<sup>TM</sup> Tissue Adhesive, St. Paul, MN, USA) with both tips free from insulation for 100  $\mu\text{m}$  were used during the preparation of electrodes for EEG recordings from all brain structures. One of wires in the electrode for EEG recordings from MC and Pt was shortened by 1 mm to simultaneously reach both brain areas. Thus, the prepared electrodes were sufficiently inflexible and had a more beneficial surface–volume ratio than a single-wire electrode of 200  $\mu\text{m}$  diameter. The reference and ground electrodes (stainless steel wire, 0.4 mm in diameter) were implanted over the caudal part of the brain (AP:  $-5.3$ ; ML:  $\pm 1.8$ ; DV:  $-0.5$ ). A computerized 3D stereotaxic StereoDrive (Neurostar, Tübingen, Germany) was used for the precise positioning of all electrodes. The latter were fixed to the skull with dental cement and soldered to a dual row socket connector (Sullins Connector Solutions, San Marcos, CA, USA). Each of the nichrom wires was soldered to one of the connector's pins. After electrode implantation, mice were housed individually for the recovery, followed by the experimental sessions and postmortem verification of the electrode tip location (see the examples and histological details in [11,12]).

## 2.2. EEG Recording

Three–four days after implantation of the electrodes, each mouse was allowed to adapt for several days (one hour per day) to the experimental environment, including an internal cage (Perspex, 15 cm  $\times$  17 cm  $\times$  20 cm) taken place in an electrically shielded chamber and a cable (five 36-gauge wires, Plexon Inc, Dallas, TX, USA) plugged in a digital Neuro-MEP amplifier (Neurosoft Ltd., Ivanovo, Russian Federation). Baseline EEG was recorded on day 8 for 30 min, starting after 20–30-min adaptation of the animal to the experimental cage. The experiments were performed during a daylight period (9:00 a.m.–6:00 p.m.), keeping the illumination at a relatively stable level by combination with an artificial light source if it was necessary.

## 2.3. EEG Coherence Computation

EEG signals were amplified, filtered (0.1–35 Hz), and sampled (1 kHz) online using the amplifier and kept in the memory of an operational computer for further analysis. The program allowed for both the automatic and manual rejection of EEG fragments containing artifacts and epileptic spikes. In the raw EEGs, evident differences in cerebral synchronization were observed between 5xFAD and WT<sub>5xFAD</sub> mice (Figure 1).

EEG data were processed using custom prepared software (see Attachment A1). Spectral coherence was estimated by averaging over 12 s epochs of baseline EEGs derived from a 1–30 Hz range, initially in a 1 Hz wide band (Figure 2).

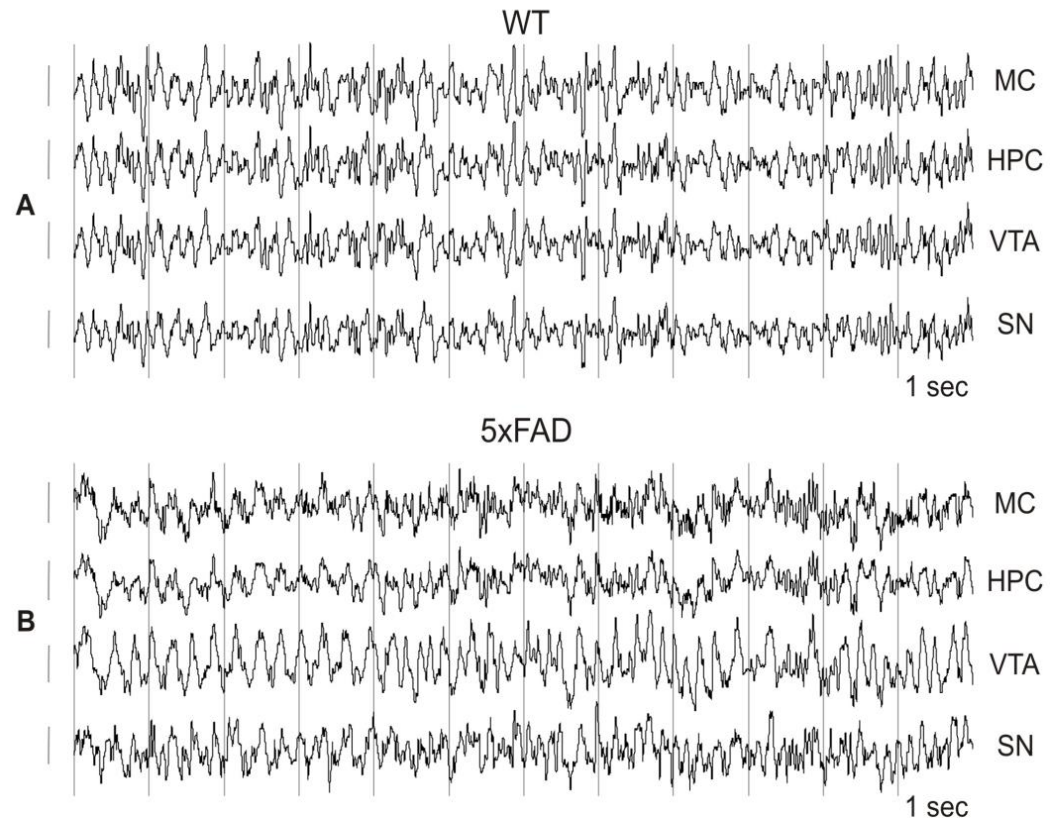
Afterwards, EEG coherence values were evaluated in the range of 1–30 Hz with the averaging of data in “classical” EEG bands (in Hz): delta 1 (1–2), delta 2 (2–4), theta (4–8), alpha (8–12 Hz), beta 1 (12–20), and beta 2 (20–30). The values of coherence in each of the frequency bands were averaged in each of the three consecutive 10 min intervals (for further statistical analysis) and for 30 min in total (for illustrations).

## 2.4. Statistics

Differences between transgenic and non-transgenic mice in the EEG coherency averaged in each of three consecutive 10 min intervals in frames of both the whole frequency spectra and individual frequency bands were analyzed by two-way ANOVA for repeated measures with Bonferroni's post hoc test for multiple comparisons (STATISTICA 10; StatSoft, Inc., Tulsa, OK, USA). All sets of data were preliminary tested on Gaussian distribution. There were 36 parameters for coherence: six “classical” frequency bands  $\times$  six combinations

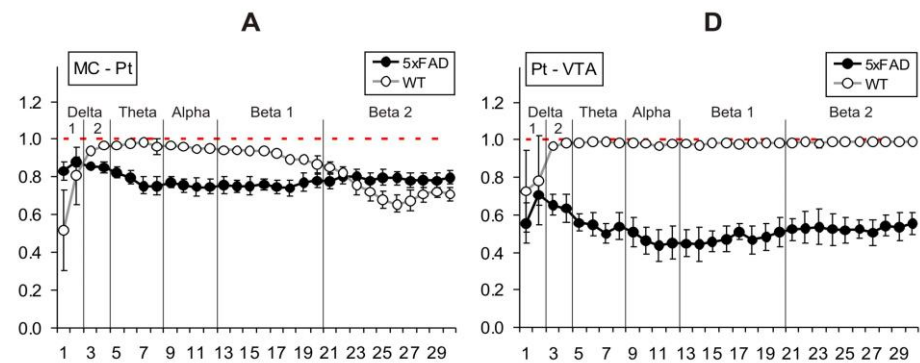
of inter-structural coherence. Results were considered statistically significant at  $p < 0.05$ . All data are shown as mean  $\pm$  SEM.

Representative 12-sec EEG fragments from 30-min baseline recordings in six-month old 5xFAD mouse and WT littermate

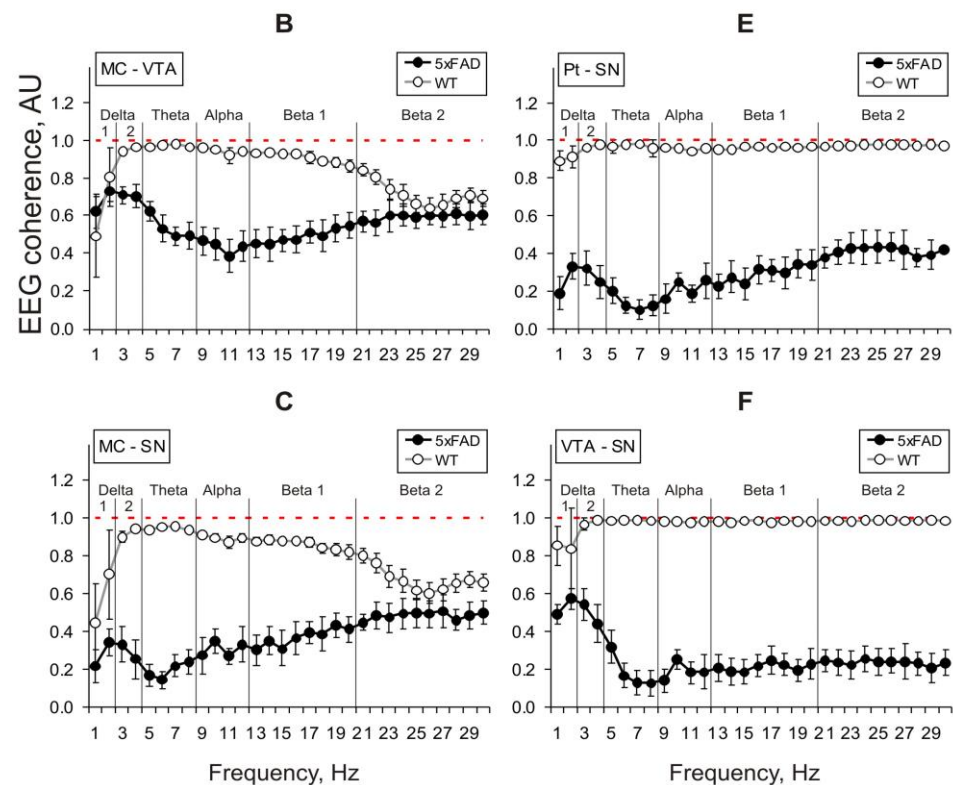


**Figure 1.** Typical patterns in 12 s fragments of baseline EEG in wakeful and behaviorally active six-month-old WT<sub>5xFAD</sub> mouse and 5xFAD littermate (A and B, respectively) in the motor cortex (MC), hippocampus (HPC), ventral tegmental area (VTA), and substantia nigra (SN). On A and B, time calibration is 1 sec, amplitude calibration is 100  $\mu$ V.

Inter-structural EEG coherence in 10-min baseline interval in six-month old 5xFAD mouse and WT<sub>5xFAD</sub> littermate



**Figure 2.** Cont.



**Figure 2.** Inter-structural coherence distributions (A–F) in six-month-old 5xFAD mouse and WT<sub>5xFAD</sub> littermate (filled and open circles, respectively) in 10 min baseline EEGs from the motor cortex (MC), hippocampus (HPC), ventral tegmental area (VTA), and substantia nigra (SN), in different frequency bands denoted on horizontal axis (abscissa). Inter-structural coherence is denoted on the plates as MC-HPC (A); MC-VTA (B); MC-SN (C); HPC-VTA (D); HPC-SN (E), and VTA-SN (F). Ordinate is the average value of EEG coherence in each of 1 Hz bands. Five vertical lines separate “classical” EEG frequency bands (from left to right: delta 1, delta 2, theta, alpha, beta 1, and beta 2, respectively). Red dashed lines show maximal coherence value.

### 3. Results

During baseline EEG recordings, the behavior of mice was typically characterized by relatively intensive exploration of the experimental box, which was occasionally alternated by short-lasting calm down periods. Baseline EEGs and their frequency compositions have been described in detail in our previous studies [11–13].

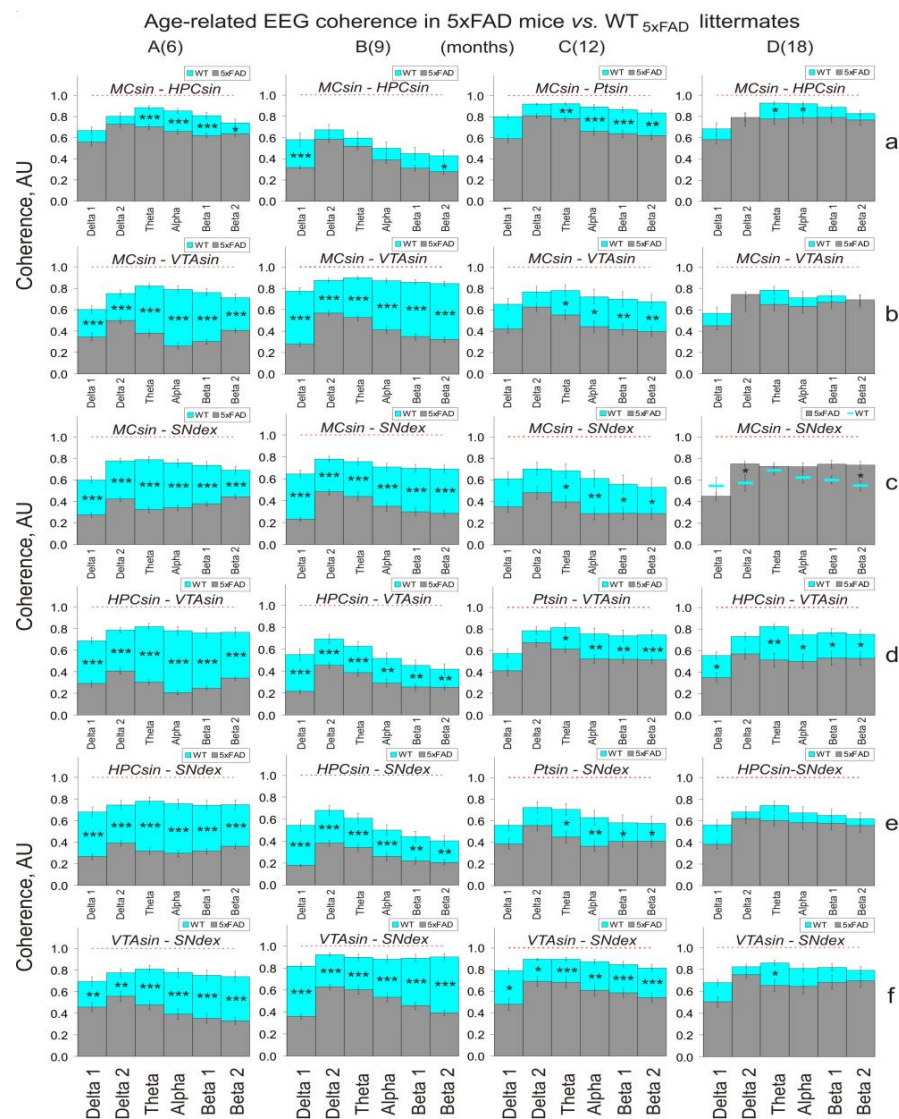
#### 3.1. EEG Coherence in 5xFAD Mice of Different Ages

Differences in the levels of EEG coherence between 5xFAD-mice and their WT<sub>5xFAD</sub> littermates were relatively stable in consecutive 10 min intervals that were readily visible in the spectral profiles of coherence averaged in the whole (30 min) baseline period that was expressed in very small values of SEMs (Figure 3).

The 5xFAD mice showed significantly lower levels of EEG coherence vs. the WT<sub>5xFAD</sub> littermates in most of the analyzed frequency bands (c.f., grey and light blue bars in Figure 3).

Evident age-related attenuation of the coherence differences between the groups was observed. The differences were significantly higher in younger mice (two-way ANOVA: (a) 6-month-old mice:  $F_{138} = 17.9, 105, 107, 163, 96.4, \text{ and } 46.3$ , for MC-HPC, MC-VTA, MC-SN; HPC-VTA, HPC-SN; and VTA-SN, respectively,  $p < 0.001$ , for all; (b) 9-month-old mice:  $F_{90} = 7.8 \text{ and } 233, 90.7, 29.2, 36.6, 115$ ,  $p = 0.006$ , for MC-HPC and  $p < 0.001$ , for others, respectively; (c) 12-month-old mice:  $F_{84} = 11.2, 11.1, 10.8, 11.5, 10.9, \text{ and } 17.7$ ,  $p = 0.001, 0.001, 0.002, 0.001, 0.001, \text{ and } <0.001$ , respectively). The coherence differences practically disappeared in the 18-month-old mice, with the exception of HPC-VTA and

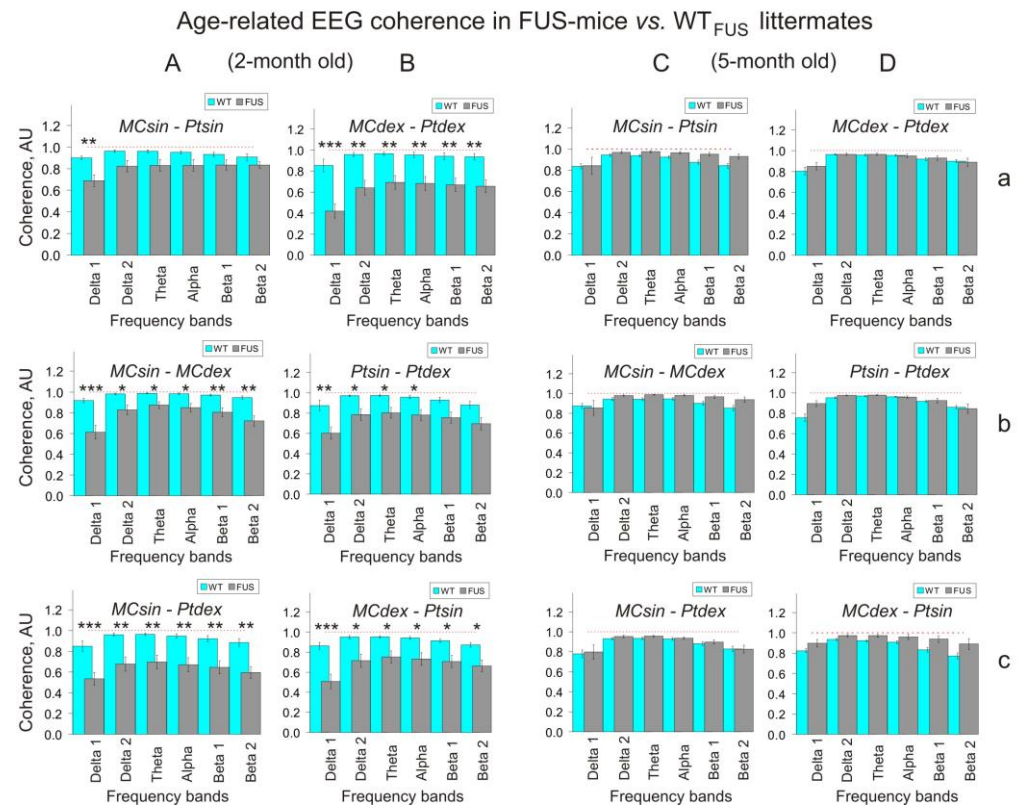
VTA-SN interrelations:  $F_{72} = 1.1, 0.3, 3.6, 13.4, 0.6,$  and  $9.4, p = 0.299, 0.588, 0.063, <0.001, 0.440,$  and  $0.003,$  respectively (Figure 3D,d; see Figure S2 for clarity). The elimination of intracerebral coherence differences between the 18-month-old 5xFAD and WT<sub>5xFAD</sub> mice was evidently associated with the age-related recovery of EEG synchrony in the transgenic mice. Indeed, at the age of 18 months, 5xFAD mice demonstrated a more significant rising of EEG coherence vs. that in the younger mice (c.f., grey bars in Figure 3D vs. Figure 3A–C; two-way ANOVA: (a) D vs. A:  $F_{96} = 13.1, 53.8, 127, 33.4, 52.1,$  and  $23,$  for MC-HPC, MC-VTA, MC-SN; HPC-VTA, HPC-SN; and VTA-SN, respectively,  $p < 0.001$  for all; (b) D vs. B:  $F_{84} = 110, 39, 97, 26.7, 69,$  and  $17.6,$  respectively,  $p < 0.001,$  for all; (c) D vs. C:  $F_{84} = 6.24, 14.9, 46, 0.04, 11.8,$  and  $2.5, p = 0.014, <0.001, <0.001, 0.846, 0.001,$  and  $0.117,$  respectively).



**Figure 3.** Age-related relations between coherence distributions in 5xFAD and WT<sub>5xFAD</sub> mice (grey and light blue bars, respectively) for 30 min baseline EEG from the motor cortex (MC), hippocampus (HPC)/putamen (Pt), ventral tegmental area (VTA), and substantia nigra (SN), in different frequency bands. Upper- and lower-case letters are used to recognize any age (A–D) and the inter-structural relations (a–f) denoted on the plates in brackets and by italic fonts, respectively. Ordinate is the average value of EEG coherence in each of the “classical” bands denoted on the horizontal axes (abscissa). Red dashed lines show maximal coherence value. Abbreviations of “sin” and “dex” indicate “left” and “right” hemispheres, respectively. Star symbols denote significant two-way ANOVA differences in separate frequency bands between 5xFAD and WT<sub>5xFAD</sub> mice, where \*, \*\*, and \*\*\* correspond to  $p < 0.05, p < 0.01,$  and  $p < 0.001,$  respectively (see Figure A1, for details).

### 3.2. EEG Coherence in FUS Mice of Two- and Five-Month Ages

The differences in the levels of EEG coherence between FUS mice and their WT<sub>FUS</sub>-littermates were relatively stable in consecutive 10 min intervals that were readily visible in the spectral profiles of coherence averaged in the whole (30 min) baseline period that was expressed in extremely small values of SEMs (Figure 4).



**Figure 4.** Age-dependent relations between coherence distributions in FUS and WT<sub>FUS</sub> mice (grey and light blue bars, respectively) for 30 min baseline EEG from symmetrical motor cortex (MC) and putamen (Pt), in different frequency bands. Upper-case letters are used to recognize FUS mice (A,C) and WT littermates (B,D) at different ages (see in brackets) and the inter-structural relations (a–c) denoted on the plates by italic fonts. Ordinate is the average value of EEG coherence in each of the “classical” bands denoted on the horizontal axes (abscissa). Abbreviations of “sin” and “dex” indicate “left” and “right” hemispheres, respectively. Red dashed lines show maximal coherence value. Star symbols denote significant two-way ANOVA differences in separate frequency bands between FUS and WT<sub>FUS</sub> mice, where \*, \*\*, and \*\*\* correspond to  $p < 0.05$ ,  $p < 0.01$ , and  $p < 0.001$ , respectively (see Figure A2, for details).

During this period, EEG coherence between MC and Pt in two-month-old FUS mice was significantly less of that in WT<sub>FUS</sub> littermates practically in all frequency bands regardless of the brain hemisphere (Figure 4A,B; two-way ANOVA:  $F_{72} = 7.3, 16.3, 21.8, 23.2, 12.7, \text{ and } 15.1$ , for Mcsin-Ptsin, Mcsin-MCdex, Mcsin-Ptdex, Mcdex-Ptdex, Ptsin-Ptdex, and Mcdex-Ptsin, respectively;  $p = 0.008$  and  $< 0.001$ , for others). Interestingly, in the FUS mice, MC-Pt coherence in the left hemisphere was significantly higher to that on the right side (c.f., grey bars in Figure 2A,B,a; two-way ANOVA:  $F_{1,84} = 7.26$ ,  $p = 0.008$ ). The EEG coherence suppression, observed in younger FUS mice, completely disappeared in the older ones (see Figures 4C,D and S2, for clarity).

## 4. Discussion

In this study, the age-related suppression of coherence between EEGs from different brain structures in both 5xFAD and FUS mice was revealed (see Figures 3 and 4, respec-

tively). This phenomenon has been shown to be characteristic for AD [17,28–30]. However, we demonstrate that the EEG coherence suppression is age-dependent, which allows the development of a “functional connectivity” approach for the studying of a role for compensatory/adaptive mechanisms in the assessment and correction of age-related AD evolution. Aging and AD are well known to be characterized by a gradual cognitive deterioration associated with modifications in the brain structures and their functional interaction [31,32] that in turn is accompanied by disturbances in neuronal synchrony [33–36]. In the aging brain, the role of the so-called “repressor element silencing transcription factor” (REST), which is well known to initiate a specific “stress-response program”, has been highlighted to be preventive for cognitive decline and AD [8,37]. The REST protein, normally expressed at low levels in the neurons of young brains, has been shown to be profoundly elevated in aged brains [8]. In 5xFAD mice, this might be linked with the age-dependent accumulation of synaptosomal mitochondrial dysfunctions [38]. In line with this suggestion, the accumulation of mitochondrial DNA deletions in dopaminergic neurons has been shown to trigger neuroprotective compensatory mechanisms [39]. In our study, the genetically programmed AD is expected to be a powerful “stressor” for the REST’s production, noticeably exceeding that in the aging process alone. Age-dependent suppression of EEG coherence in 5xFAD mice (see Figure 3) seems to characterize the REST involvement in a recovery of interrelations between the affected brain structures up to those in control 18-month-old WT<sub>5xFAD</sub> mice. Residual suppression of HPC-VTA coherence in 5xFAD mice at this age (Figure 3d,D) highlights enhanced susceptibility of interrelations between these structures to AD-associated pathological disturbances in the brain. Given the important modulatory role of VTA in the switching of HPC from inhibition to the enhancement of its information flow [40], the residual suppression of EEG coherence between VTA and HPC might be a part of age-related mechanisms of cognitive impairment in AD [41]. The suppressed EEG synchrony/coherence between VTA and SN are seemingly linked with the age-related loss of dopaminergic neurons in these areas, where a statistically significant effect has been shown to start from 9 months of age [41]. A similar phenomenon was observed in WT<sub>5xFAD</sub> (C57BL/6) littermates [24]. The age-related expansion of microglia into the dopamine-producing areas is directed to increase dopamine neuron surveillance by compensating for the progressive decline in morphological complexity (senescence) of microglia [42,43]. Thus, an association of senescent cells, brain plasticity and impairments in cognition might be an attractive target for further studies of interrelations between mechanisms of aging and AD [44].

In younger (two-month-old) FUS mice vs. control WT<sub>FUS</sub> (CD-1) littermates, evident EEG coherence suppression was observed in all cortex–putamen combinations (see Figure 3A,B). In older transgenic mice, the coherence profiles were practically identical to those in non-transgenic ones (see Figure 3C,D). This is in line with the suggestion that a combination of circuits with different connectivity is characteristic for an involvement of neurodegenerative and adaptive mechanisms in ALS development [21]. Interestingly, in two-month-old FUS mice, EEG coherence between MC and Pt in the left hemisphere was noticeably higher than that on the right side (c.f., Figure 4a,A vs. Figure 4B), despite the lacking differences in interhemispheric asymmetry separately in the cortices and putamen (c.f., Figure 4b,A,B, respectively). This early characteristic of ALS might be explained by the impairment of coupled structural and functional connectivity during the development of the disease [45], thus highlighting the role of cortico–striatal interrelations in age-related ALS mechanism(s). On the other hand, this allows the development of a special asymmetry-based approach for the differentiation of ALS from other neurodegenerative pathologies. The intimate age-related mechanisms of ALS pathogenesis seem to be linked with a fine balance in the expression of inflammation-associated factors that in turn affects the developmental profile of disease and survival [46,47]. EEG coherence recovery in five-month-old FUS mice to control values (Figure 4C,D) is in line with protective microglia functions from ALS-related degeneration that is observed, in particular, in TDP-43 mice, one of the ALS models [48].



In spite of evident total suppression of EEG coherence in younger 5xFAD and FUS mice, some peculiarities revealed in this study might be preliminarily analyzed. Shortly, different levels of coherence between EEGs from the brain areas in WT<sub>5xFAD</sub>- and WT<sub>FUS</sub>- mice (c.f., light blue bars in Figures 3 and 4) appear to be associated with different temporal patterns of involvement of pro- and anti-inflammatory factors in mechanisms of adaptation in mice of different phenotypes (C57BL/6J and CD-1, respectively). Secondly, suppressed EEG coherence between MC and Pt in the right vs. left hemispheres in two-month-old FUS mice (c.f., grey bars in Figure 4a,B vs. Figure 4A, respectively) highlights the significance of intra-hemispheric functional interrelations in addition to inter-hemispheric asymmetry shown in other ALS studies [25]. Interestingly, no interhemispheric asymmetry was separately observed for MC and Pt in our study (c.f., grey bars in Figure 4b,A,B). Finally, evidently less EEG coherence between HPC and other brain areas in nine-month-old WT<sub>5xFAD</sub> mice (c.f., Figure 3a,d,e,B vs. Figure 3A,C,D) highlights an age dependence of a role of HPC in the brain functioning, specifically, of cognitive mechanisms in mice [24].

## 5. Conclusions

Our data highlight a crucial role of age-related adaptive mechanisms in the modification/elimination of intracerebral disturbances associated with neurodegenerative pathologies (AD and ALS, in particular). We demonstrate that intra-cerebral coherence measurements allow the revealing of the pathologies, their differentiation, and progression. This approach is apparently useful and effective for the understanding of the inter-structural mechanisms involved in the development of neurodegenerative processes of different etiologies. In this respect, further detailed analysis of a role for frequency-specific EEG oscillations in the functional coupling of different brain areas has a great potential for the understanding of the interconnected mechanisms of adaptation and pathology.

**Supplementary Materials:** The following supporting information can be downloaded at <https://www.mdpi.com/article/10.3390/biomedicines11041151/s1>, Figure S1—Short description of custom prepared soft for calculation of EEG coherence function; Figure S2—Age-related differences between EEG coherence distributions in 5xFAD and WT<sub>5xFAD</sub> mice estimated by two-way ANOVA; Figure S3—Age-related differences between EEG coherence distributions in FUS and WT<sub>FUS</sub> mice estimated by two-way ANOVA. Refs. [49–51] are cited in the supplementary materials.

**Author Contributions:** Conceptualization and methodology, V.V.; soft and formal analysis, A.D.; investigation, K.C.; resources, A.A.U.; data curation, V.V. and E.L.; writing—original draft preparation, V.V. All authors have read and agreed to the published version of the manuscript.

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**Institutional Review Board Statement:** The animal study protocols were approved by the local institute's ethics review committee (protocols: No. 30, 30.04.2019 and No. 52, 18.09.2020). All animal work was carried out in accordance with the "Guidelines for accommodation and care of animals Species-specific provisions for laboratory rodents and rabbits" (GOST 33216-2014) in compliance with the principles enunciated in the Directive 2010/63/EU on the protection of animals used for scientific purposes.

**Informed Consent Statement:** Not applicable.

**Data Availability Statement:** Data are contained within the current article and its Supplementary Material.

**Conflicts of Interest:** The authors declare no conflict of interest.

## Appendix A

Brain Areas	MCsin-HPCsin (A)							
	6		9		12		18	
Age, Months	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	3.6	0.063	13.9	<0.001	1.2	0.290	0.2	0.643
delta2	2.3	0.137	2.5	0.124	0.2	0.681	0.7	0.403
theta	30.8	<0.001	1.4	0.243	7.6	0.008	5.4	0.026
alpha	24.1	<0.001	2.2	0.144	14.2	<0.001	4.6	0.039
beta1	16.8	<0.001	3.8	0.057	15.0	<0.001	2.4	0.130
beta2	4.4	0.041	5.1	0.030	12.1	0.001	0.3	0.563

Brain Areas	MCsin-VTAsin (B)							
	6		9		12		18	
Age, Months	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	20.8	<0.001	150	<0.001	3.4	0.071	0.4	0.508
delta2	20.7	<0.001	79.5	<0.001	0.1	0.752	2.9	0.098
theta	87.6	<0.001	85.9	<0.001	4.3	0.043	1.6	0.215
alpha	103	<0.001	90.2	<0.001	6.8	0.012	0.4	0.534
beta1	84.7	<0.001	132	<0.001	8.6	0.005	0.3	0.607
beta2	38.1	<0.001	173	<0.001	9.9	0.003	0.1	0.756

Brain Areas	Mcsin-SNdex (C)							
	6		9		12		18	
Age, Months	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>42</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	47	<0.001	89.7	<0.001	3.4	0.074	0.2	0.661
delta2	86.8	<0.001	48.8	<0.001	1.4	0.242	5.2	0.028
theta	85.7	<0.001	26.5	<0.001	7.2	0.010	0.7	0.395
alpha	59.5	<0.001	30.1	<0.001	9.5	0.004	1.7	0.203
beta1	45.8	<0.001	45.9	<0.001	6.6	0.014	3.4	0.074
beta2	20.7	<0.001	62.9	<0.001	6.0	0.019	5.4	0.026

Brain Areas	HPCsin-VTAsin (D)							
	6		9		12		18	
Age, Months	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>
delta1	63.9	<0.001	33.9	<0.001	1.1	0.293	6.13	0.018
delta2	80	<0.001	18.7	<0.001	0.8	0.377	1.94	0.172
theta	122	<0.001	15.2	<0.001	7.3	0.009	12.3	0.001
alpha	114	<0.001	11.3	0.002	7.7	0.008	6.25	0.017
beta1	79.3	<0.001	10.0	0.003	9.6	0.003	6.54	0.015
beta2	49.6	<0.001	7.9	0.007	14.5	<0.001	5.2	0.029

Brain Areas	PCsin-SNdex (E)							
	6		9		12		18	
Age, Months	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>
delta1	43.6	<0.001	46.8	<0.001	3.3	0.076	2.6	0.113
delta2	38.5	<0.001	25.8	<0.001	3.5	0.068	0.1	0.774
theta	74.2	<0.001	15.0	<0.001	4.4	0.042	1.2	0.282
alpha	56.5	<0.001	13.5	<0.001	9.2	0.004	0.5	0.492
beta1	46.3	<0.001	12.1	0.001	4.6	0.038	0.2	0.672
beta2	35.2	<0.001	10.5	0.002	4.1	0.048	0.8	0.783

Figure A1. Cont.

Brain Areas	VTAsin-SNdex (F)							
	6		9		12		18	
Age, Months								
Bands/Coherence	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>	F <sub>69</sub>	<i>p</i>	F <sub>45</sub>	<i>p</i>
delta1	11.6	0.001	95.7	<0.001	4.2	0.046	4.0	0.545
delta2	10.8	0.001	70.4	<0.001	4.6	0.038	0.5	0.468
theta	29.4	<0.001	24.2	<0.001	14.4	<0.001	6.4	0.018
alpha	27.7	<0.001	34.1	<0.001	9.9	0.003	3.3	0.077
beta1	29.8	<0.001	62.9	<0.001	14.1	<0.001	1.8	0.185
beta2	34.2	<0.001	129	<0.001	17.1	<0.001	0.8	0.392

Figure A1. Two-way ANOVA analysis of EEG coherence in separate frequency bands between various brain areas (A–F) in 5xFAD vs. WT<sub>5xFAD</sub> mice of different ages (6, 9, 12, 18 months).

Brain Areas	MCsin-Ptsin (A)				MCdex-Ptdex (B)			
	2		5		2		5	
Age, Months								
Bands/Coherence	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	7.4	0.001	0.1	0.773	25.1	<0.001	0.0	0.962
delta2	2.6	0.116	0.2	0.701	10.5	0.003	1.1	0.305
theta	0.8	0.385	0.1	0.817	9.3	0.004	0.9	0.342
alpha	1.6	0.213	0.1	0.790	8.4	0.006	1.2	0.272
beta1	0.3	0.629	0.3	0.619	8.7	0.006	0.5	0.475
beta2	0.1	0.800	0.3	0.601	9.6	0.004	1.1	0.309

Brain Areas	MCsin-MCdex (C)				Ptsin-Ptdex (D)			
	2		5		2		5	
Age, Months								
Bands/Coherence	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	13.2	<0.001	1.8	0.194	12.4	0.001	0.0	0.973
delta2	6.2	0.018	1.2	0.277	5.4	0.026	1.8	0.184
theta	6.0	0.019	0.7	0.399	4.9	0.033	2.4	0.127
alpha	6.5	0.015	0.1	0.790	4.4	0.043	3.0	0.094
beta1	8.1	0.007	0.3	0.600	3.7	0.062	2.5	0.122
beta2	11	0.002	0.1	0.783	3.3	0.076	3.0	0.091

Brain Areas	MCsin-Ptdex (E)				MCdex-Ptsin (F)			
	2		5		2		5	
Age, Months								
Bands/Coherence	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>	F <sub>36</sub>	<i>p</i>
delta1	17.2	<0.001	0.6	0.432	13.9	<0.001	0.4	0.508
delta2	9.0	0.005	1.9	0.174	7.1	0.011	1.4	0.242
theta	8.1	0.007	1.7	0.196	6.0	0.019	0.8	0.390
alpha	7.7	0.009	2.4	0.130	6.0	0.019	0.8	0.374
beta1	8.3	0.007	1.8	0.191	6.3	0.017	0.0	0.911
beta2	10.3	0.003	2.3	0.136	7.1	0.012	0.0	0.957

Figure A2. Two-way ANOVA analysis of EEG coherence in separate frequency bands between various brain areas (A–F) in FUS vs. WT<sub>FUS</sub> mice of different ages (2 and 5 months).

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